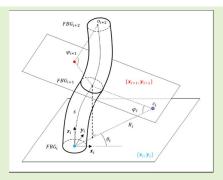


3D Shape Sensing With Multicore Optical Fibers: **Transformation Matrices Versus Frenet-Serret Equations for Real-Time Application**

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Abstract—This paper presents the characterization of an algorithm aimed at performing accurate fiber optic-based shape sensing. The measurement of the shape relies on the evaluation of the strains applied to an optic fiber in order to identify relevant spatial parameters, such as the curvature radii and bending direction, which define its shape. The measurement system is based on a 7-core multicore fiber, containing up to 9 triplets of fiber Bragg grating sensors (FBGs) organized around a central core used as reference. The proposed study aims at comparing the widely used Frenet-Serret equations with an algorithm based on the homogeneous transformation matrices that are normally used in robotics to express the position of a point in different frames, i.e. from



local to global coordinates. The numerical results of the performed experiments (with different multicore fibers and setups) extensively prove the superiority of the alternative method over the Frenet-Serret equations in terms of finding a trade-off between accuracy and execution time.

Index Terms—Shape sensing, fiber Bragg grating, multicore optical fiber, homogeneous transformation matrix, Frenet-Serret, performance, three-dimensional.

I. INTRODUCTION

HAPE measurement is an essential part of the sensing field, which has been receiving a lot of interest in the past few decades. Conventional shape sensors are divided into two groups: non-contact based and contact-based sensors [1]. Non-contact sensors rely on different approaches, such as magnetic-based tracking techniques, structured illumination, 3D cameras and image-based techniques [1]-[6]. Contact sensors are mostly based on electrical resistivity and strain sensors, micro-electromechanical systems, and optoelectronic

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measurements [7]-[9]. One of the more challenging application of shape sensing is in those cases where non-contact visual systems are not viable, and accurate realtime information of the shape of a dynamic object is needed.

Amongst the contact sensors, optical fiber sensors have attracted a specific interest due to their unique advantages, such as immunity to external electromagnetic fields, small dimensions (40-250 μ m diameter), low mass, ease of attachment, robustness and multiplexing capabilities [10]–[12]. These properties allow the fiber optic sensors to be easily embedded in the object to be monitored, and require a single remote interrogator unit, without the complexity of wiring several sensors.

Fiber optic shape sensing is mainly based on multi-dimensional bend measurements along the sensing fiber, that can be distributed [13], [14] and quasi-distributed [15]. Distributed strain sensing relies on two light scattering phenomena: Rayleigh and Brillouin scatterings. Sensing based on Rayleigh scattering is able to measure only relative changes of strain because it analyses the spectral shift between a new measurement and the reference measurement (without strain applied) [16]. Brillouin-based sensing, on the other hand, can be used for absolute measurements since it utilizes a linear relationship between the applied strain and the energy of the acoustic phonons [17]. All distributed sensing techniques are mainly limited by the low scanning

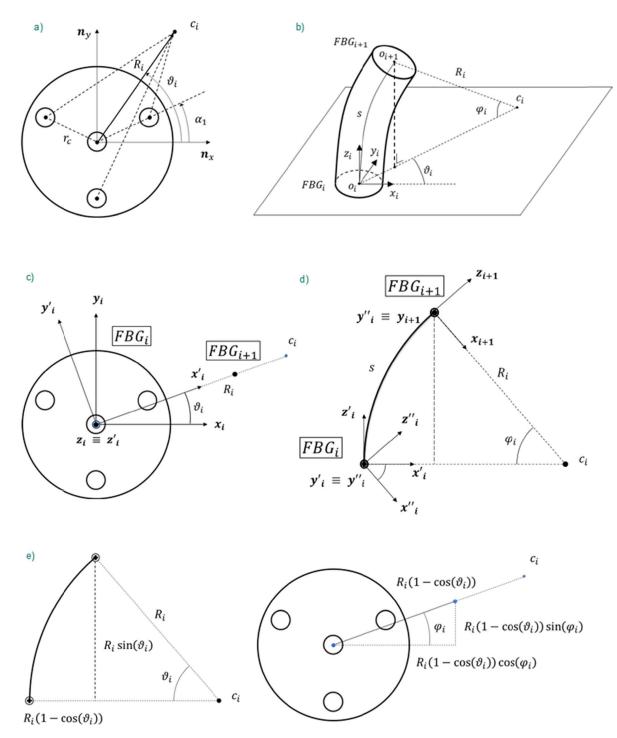


Fig. 1. Shape reconstruction algorithm based on homogenous transformation matrices. a) FBG_i section view, n_x , n_y plane - the information from the outer cores allow for the calculation of the curvature vector of the overall fiber. The angle α_i (i=1,2,3) locates the position of the cores with respect to versor n_x . b) From FBG_i to FBG_{i+1} - location o_{i+1} is identified starting from o_i with the knowledge of ϑ_i , R_i and triplet x_i , y_i , z_i . c) FBG_i section view, x_i , y_i plane - FBG_i senses a curvature radius R_i and an azimuth angle ϑ_i , which identify an in-plane rotation center c_i . FB G_{i+1} is out of the considered section plane. The first passage consists in aligning the x axis with the rotation center c_i . d) Multicore fiber, external side view, x_i' , z_i' plane - FBG_{i+1} is located by performing a circular motion of length s (FBG distance) around center c_i starting from FBG_i . The angle φ_i is obtained from the known parameters R_i and s, and is used to re-align the x axis towards the rotation center c_i . e) From FBG_i to FBG_{i+1} - location o_{i+1} is identified starting from o_i with the knowledge of ϑ_i , R_i and triplet x_i, y_i, z_i .

rate and the high cost of the interrogation devices for practical applications.

Quasi-distributed fiber optic shape sensing relies on fiber Bragg grating (FBG) strain measurements. FBG results from

a periodic modulation of the refractive index in the fiber core, that strongly reflects a specific wavelength, called the Bragg wavelength, when broadband light is incident on it [18]. This characteristic wavelength is function of the grating period

(the distance between two consecutive high-index regions) and the effective refractive indices of two high-index regions, that, in their turn, are changed when mechanical strain or temperature is applied to the grating. As a result, the Bragg wavelength monitoring allows point strain or temperature measurement. Also, multiple FBGs (FBG array) with different grating periods can be used along the same fiber to have a quasi-distributed strain measurement. In this case, a wavelength division multiplexing (WDM) property is used, i.e., the set of different reflected Bragg wavelengths is analysed to measure strain values at spatially distributed gratings. The high sampling rates (up to 10 kHz) and lower costs of the interrogation devises for FBG measurements make quasi-distributed shape sensing more suitable for real-time applications [19].

Since FBG-based shape sensing provides quasi-distributed strain data along the fiber, local position and orientation of the fiber are obtained at discrete points. This discreteness of the measurements can introduce mathematical errors in the results of shape reconstruction. Two possible ways to reduce these errors are: (a) the use of highly dense FBG arrays or (b) interpolation of the real measured data on a larger number of points. The first approach is limited by the WDM capabilities of the interrogation device and the FBG array. i.e., the limited amount of Bragg wavelengths that can be in the wavelength range of the interrogator. As a result, the FBG array has a trade-off between spatial resolution and sensing length of the array. The second approach with interpolation of the real data solves the WDM limitation problem and decreases the mathematical errors of the reconstruction. However, the increase of data sets decreases the speed of real-time shape reconstruction yielding a trade-off between accuracy and performance of reconstruction. As a result, the search for an algorithm for shape reconstruction optimized for specific applications becomes relevant.

The Frenet-Serret equations constitute the most popular approach for description of curves in three-dimensional space [15], [20]–[22], but are affected by implementation errors, which can influence the final reconstruction accuracy. In particular, the vectors of the reference frame do not maintain unitary norm due to the aforementioned implementation errors, and the movements in the direction of the current tangent vector are linear, whereas the actual shape of the fiber is a curve. These errors can be reduced by simulating a more spatially resolved set of measurements, which can be accomplished by interpolating the real data on a larger number of points. Because the amount of mathematical operations directly depends on the dataset size, accuracy and computational performance are in conflict.

In this work we use the same concepts already introduced by Roesthuis *et al.* [32] and report an alternative shape reconstruction algorithm based on homogenous transformation matrices. The performances of the algorithm are then thoroughly analysed by comparing them with the ones obtained with the equations of Frenet-Serret, which are the most widespread technique currently in use for shape sensing with multicore optical fibers. A 3D shape measurement system based on FBG arrays inscribed into a 7-core optical fiber by femtosecond

laser inscription technique [23] was used to perform the experiments and assess the algorithm performances.

II. ALGORITHM

A. Estimation of Curvature From Measured Strain

The directional strain values measured by the array of FBG triplets inscribed in the fiber (e.g. [15], [24]) are the input quantities of the reconstruction algorithm. The relationship that has been used to retrieve the strain values ε_i from the measured shifts in Bragg wavelengths of spectra, is:

$$\Delta \lambda_i / \lambda_{B,i} = C_i \cdot \varepsilon_i \tag{1}$$

where i is the index of the grating, $\lambda_{B,i}$ is the Bragg wavelength in initial conditions (absence of bending-induced strain), $\Delta \lambda_i$ is the Bragg wavelength shift and C_i is the static sensitivity of the sensing system to ε [15]. The chain of FBGs within the central core experiences almost no bending-induced strain, which results into $\Delta \lambda_i \sim 0$. For this reason, the signals measured by the FBGs within the fiber core were subtracted from the wavelength shifts of the FBGs in the side cores, for compensating the effect of longitudinal strain and temperature on the calculated curvature. In order to achieve more accurate results, the strain data is interpolated with the piecewise cubic Hermite function; the interpolation coefficient (factor) m will be used to denote the number of additional segments in which every FBG-to-FBG portion is furtherly divided. For example, an interpolation coefficient m = 2 for an array of 6 FBGs implies a total number of evaluated points equal to (m-1). 5+6=11. While spline interpolation is smoother and more accurate if the data represents values of a smooth function, piecewise cubic Hermite interpolation has no overshoots and yields a result with less oscillations [25], [26].

The curvature vector κ is then calculated from the strain values, according to [13], with the following formula:

$$\kappa_{i} = -\frac{2}{Nr_{c}} \left(\sum_{i=1}^{N} \varepsilon_{i} \cos \alpha_{i} n_{x} + \sum_{i=1}^{N} \varepsilon_{i} \sin \alpha_{i} n_{y} \right)$$
 (2)

where N is the number of cores, r_c is the core distance from the fiber center, n_x and n_y are the components of the two arbitrarily decided vectors that define the plane where the FBG triplet lies and α_i is the angle between n_x and the i-th core, as shown in Fig. 1a. Curvature modulus and angle are retrieved from the curvature vector κ . Here, the radius R is calculated as the inverse of curvature modulus κ , whereas the angle ϑ is defined as the phase of the two components of vector κ . Starting from (2), the following sensing techniques can be developed.

B. Homogeneous Transformation Matrices

The shape-reconstructing method utilizes homogenous transformation matrices, useful to express the coordinates of a point in a different frame, as described in (3):

$$\tilde{p}_{i+1}^{i} = \begin{bmatrix} p_{i+1,x}^{i} \\ p_{i+1,y}^{i} \\ p_{i+1,z}^{i} \\ 1 \end{bmatrix} = A_{i+1}^{i} \tilde{p}_{i+1}^{i+1} = \begin{bmatrix} R_{i+1}^{i} & o_{i+1}^{i} \\ \mathbf{0}_{3}^{T} & 1 \end{bmatrix} \tilde{p}_{i+1}^{i+1}$$
(3)

where \tilde{p}_{i+1}^{l} are the homogeneous coordinates of FBG_{i+1} with respect to the reference frame located at FBG_i , $p_{i+1,k}^i$ with $k = \{x, y, z\}$ is the k_{th} component of position $\tilde{p}_{i+1}^i A_{i+1}^i$ is the homogeneous transformation matrix from frame i + 1 to frame i and \tilde{p}_{i+1}^{i+1} are the homogeneous coordinates of FBG_{i+1} with respect to the reference frame located at FBG_{i+1} itself, which correspond to the origin $[0001]^T$. Homogenous transformation matrices always exhibit the same inner structure: \mathbf{R}_{i+1}^{i} is a 3×3 rotation matrix that aligns the orientation of the two considered frames, o_{i+1}^i is the origin of frame i+1 expressed in frame i and $\mathbf{0}_3^T$ is a 1×3 null vector.

This change of coordinates will be adopted during the shape reconstruction to express all the FBG positions in the starting frame, with the aid of the property reported in the following equation:

$$\tilde{\mathbf{p}}_{i+1}^{0} = \mathbf{A}_{1}^{0} \mathbf{A}_{2}^{1} \cdots \mathbf{A}_{i}^{i-1} \mathbf{A}_{i+1}^{i} \tilde{\mathbf{p}}_{i+1}^{i+1} = \mathbf{A}_{i+1}^{0} \tilde{\mathbf{p}}_{i+1}^{i+1} \tag{4}$$

It is hereafter considered a cross-section of the fiber located at the i^{th} FBG location (Fig. 1b). The frame, represented by the unitary triplet $\{x_i, y_i, z_i\}$, is rotated around z_i of an angle ϑ_i (Fig. 1c) and around y'_i of an angle φ_i (Fig. 1d).

The corresponding rotation matrices used to align the i-th frame with the (i+1)-th frame are reported in (5) and (6).

$$\mathbf{R}_{z_i}(\vartheta_i) = \begin{bmatrix} \cos(\vartheta_i) & -\sin(\vartheta_i) & 0\\ \sin(\vartheta_i) & \cos(\vartheta_i) & 0\\ 0 & 0 & 1 \end{bmatrix}$$

$$\mathbf{R}_{y_i'}(\varphi_i) = \begin{bmatrix} \cos(\varphi_i) & 0 & \sin(\varphi_i)\\ 0 & 1 & 0\\ -\sin(\varphi_i) & 0 & \cos(\varphi_i) \end{bmatrix}$$

$$(5)$$

$$\mathbf{R}_{\mathbf{y}_{i}'}(\varphi_{i}) = \begin{bmatrix} \cos(\varphi_{i}) & 0 & \sin(\varphi_{i}) \\ 0 & 1 & 0 \\ -\sin(\varphi_{i}) & 0 & \cos(\varphi_{i}) \end{bmatrix}$$
(6)

The origin of frame i + 1 with respect to frame i is obtained with the following trigonometric formula, as it is clearly shown in Fig. 1e:

$$\boldsymbol{o}_{i+1}^{i} = \begin{bmatrix} R_{i} \left(1 - \cos\left(\varphi_{i}\right)\right) \cos\left(\vartheta_{i}\right) \\ R_{i} \left(1 - \cos\left(\varphi_{i}\right)\right) \sin\left(\vartheta_{i}\right) \\ R_{i} \sin\left(\varphi_{i}\right) \end{bmatrix}$$
(7)

Equation (3) can be rewritten by including the information from (5), (6) and (7):

$$\tilde{\boldsymbol{p}}_{i+1}^{i} = \boldsymbol{A}_{i+1}^{i} \tilde{\boldsymbol{p}}_{i+1}^{i+1} = \begin{bmatrix} \boldsymbol{R}_{z_{i}} (\vartheta_{i}) \boldsymbol{R}_{y_{i}'} (\varphi_{i}) & \boldsymbol{o}_{i+1}^{i} \\ \boldsymbol{o}_{3}^{T} & 1 \end{bmatrix} \tilde{\boldsymbol{p}}_{i+1}^{i+1}$$
(8)

The complete inner structure of the homogenous transformation matrix is the following:

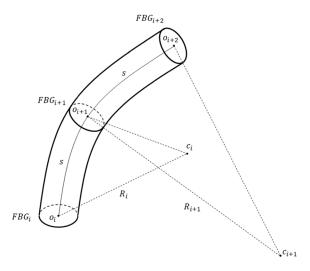
$$A_{i+1}^{i} = \begin{bmatrix} \cos(\vartheta_{i})\cos(\varphi_{i}) & -\sin(\vartheta_{i}) \\ \sin(\vartheta_{i})\cos(\varphi_{i}) & \cos(\vartheta_{i}) \\ -\sin(\varphi_{i}) & 0 \\ 0 & 0 \end{bmatrix}$$

$$\frac{\cos(\vartheta_{i})\sin(\varphi_{i})}{\sin(\vartheta_{i})\sin(\varphi_{i})} \frac{R_{i}(1-\cos(\varphi_{i}))\cos(\vartheta_{i})}{R_{i}(1-\cos(\varphi_{i}))\sin(\vartheta_{i})}$$

$$\frac{\cos(\varphi_{i})}{\cos(\varphi_{i})} \frac{R_{i}\sin(\varphi_{i})}{R_{i}\sin(\varphi_{i})}$$

$$(9)$$

An approximation is introduced in this method: the curvature radius R_i is assumed to be constant along the considered arc, whereas Fig. 2 shows that at location i+1 the actual value is R_{i+1} Despite that, when the distance between two locations



External view of the fiber. While the change of curvature is Fig. 2. continuous along the length of the fiber, the information is available only at discrete points (FBG locations). The values of curvature between two contiguous FBGs are obtained with data interpolation.

is small enough, the difference between R_i and R_{i+1} becomes negligible. An approach useful to reduce the potential error deriving from this approximation is based on the interpolation of the measured data on a larger number of virtual points along the length of the fiber, simulating a distributed FBG-based fiber.

C. Frenet-Serret Equations

The same result achieved with Frenet-Serret can be obtained with the proposed algorithm, but with less virtual sensors (related to the interpolation factor m), as it will be shown in Section IV. As a reference for further discussion, the standard Frenet-Serret equations are reported below for clarity [24]:

$$N(i) = \frac{s\tau(i) \mathbf{B}(i-1) - s\kappa(i) \mathbf{T}(i-1) + N(i-1)}{1 + s^2\tau^2(i) + s^2\kappa^2(i)}$$

$$\mathbf{T}(i) = s\kappa(i) N(i) + \mathbf{T}(i-1)$$

$$\mathbf{B}(i) = -s\tau(i) N(i) + \mathbf{B}(i-1)$$

$$\mathbf{r}(i) = s\mathbf{T}(i) + \mathbf{r}(i-1)$$
(10)

where i is an integer representing the discrete location of the curve we are considering, corresponding to distance s * ifrom the beginning, s represents the distance between two consecutive FBGs (which are virtual if data interpolation was performed), r(i) is the vector of the positions corresponding to the i-th FBG. $\{T(i), N(i), B(i)\}\$ is a triplet of orthogonal unitary vectors defined as the tangent (T), normal (N) and binormal (B) vectors to the curve, abbreviated as **TNB** triplet.

The Frenet-Serret equations reported in (10) belong to the discrete domain and are presented in a form that can be accepted by a software that executes operations in a sequential order (i.e. MATLAB).

The scalar functions τ (i) and κ (i) are the torsion and the curvature of the shape; function $\kappa(i)$ is the same reported in (2) whereas the torsion function is defined as:

$$\tau(i) = (\vartheta(i) - \vartheta(i-1))/s \tag{11}$$

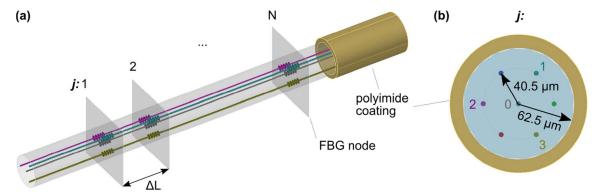


Fig. 3. Multicore fiber. Schematic representation of a 3D FBG array inscribed in the polyimide-coated 7-core optical fiber: a) 3D view and b) transverse section.

The Frenet-Serret equations assume s to be infinitesimal and the curve to always be well defined (curvature radius $R < \infty$) so that the triplet **TNB** can be univocally defined. An infinitesimal s can be achieved with a sufficiently large interpolation factor m, which creates a wider set of virtual FBGs with shorter distance between each other. On the other hand, because the fiber can be straight in certain points or segments, a curvature cannot be always guaranteed. Nonetheless, some techniques or variations can be implemented to prevent this situation (e.g., parallel transport [27], negative curvature [28]).

III. MULTICORE FIBER AND EXPERIMENTAL SETUP

In order to evaluate the performance of the above-described algorithms, 3D FBG arrays contained in a polyimide-coated 7-core optical fiber manufactured by the Fiber Optics Research Center (Moscow, Russia) were used. The fiber has seven identical straight cores – the central one and six surrounding side cores located in the corners of a regular hexagon. The distance between the cores is 40.5 μ m, the cladding diameter is 125 μ m, and the mode field diameter for each core is 5.7 μ m at 1550 nm. The fiber is coated with a 15 μ m thick polyimide layer, thus giving the outer fiber diameter of 154 μ m. To couple optical signals into separate cores, a matching fan-out device was used. The polyimide protective coating of the fiber provides the high mechanical strength and the high-temperature resistance (short term up to 400 °C and continuous operation at 300 °C) in comparison with acrylate one (up to 85 °C) [23], [29]. These properties make this sensor well-suited for harsh environments or for some medical and composite material applications.

To fabricate an FBG array the femtosecond plane-by-plane method was used, which is based on focusing an astigmatic femtosecond beam in the region of a fiber core [15]. In the case under study the infrared femtosecond pulses are produced by Light Conversion Pharos 6W l (wavelength $\lambda=1030$ nm, pulse duration $t_p=232$ fs, and pulse repetition rate f=1 kHz). In order to focus femtosecond pulses into the fiber it was used a Mitutoyo 50X Plan Apo NIR HR objective (NA = 0.65) and an additional cylindrical lens with a focal distance $f_c=-1000$ mm, mounted before the objective. A special glass ferrule with polished side faces makes it possible to fix the transverse position of the multicore fiber

with respect to the focal point [30]. The longitudinal periodic modulation of the refractive index is achieved by moving the fiber with a predefined constant velocity $v_{tr} \approx 1$ mm/s (2nd order of Bragg resonance), by using an Aerotech ABL1000 high-precision air-bearing linear stage. Thus, the FBG period is determined by $\Lambda = v_{tr}/f$, and the resonant wavelength by $\lambda_B = 2n_{eff}v_{tr}/(mf)$, where m=2 is the order in which resonant reflection of the optical signal on the FBG structure is realized. The end of the fiber, threaded through the ferrule, is fixed on the linear stage with the help of a clamp with an angular degree of freedom allowing to turn the fiber around its axis. Inscription of FBGs in the multicore fiber was carried out through the polyimide coating.

Two different multicore fibers were used in the experiments in order to show the independency of the algorithm properties from the specific fiber under test.

The first one (fiber #1) consists of 6 nodes along the fiber with an interval between the centers of the adjacent nodes $\Delta L_1 = 14$ mm, and the second one (fiber #2) consists of 9 nodes along the fiber with an interval between the centers of the adjacent nodes $\Delta L_2 = 10$ mm. In each node, uniform FBGs with a constant length $L_{FBG} = 2$ mm were inscribed in the central core, and in three side cores located at the corners of an equilateral triangle. Thereby the total length of fiber #1 was $L_1 = 72$ mm, and the total length of fiber #2 was $L_2 = 82$ mm. A schematic representation of the created fibers, as well as the FBG numbering in the arrays, is shown in Fig. 3. Uniform distribution of FBG resonant wavelengths along the same core is ensured by sequential variation of FBG periods.

To interrogate the fabricated multicore fibers, the HBM FS22-SI 8-channel interrogation unit (wavelength range from 1500 nm to 1600 nm, Fig. 4) was used. The processing of the measured spectra, detection and tracking of the FBG reflection peaks, was maintained with the BraggMONITOR SI application. More information about the procedure of the shape sensor calibration and relevant data can be found in [15].

When reconstructing the fiber shape, different curves were analysed, including different 2D bow-like and s-like curves, and a 3D spiral wound onto a surface of cylinder. In order to diminish possible torsions, the straight section of the fiber containing an FBG array was glued with adhesive tape and then taped to a sheet of scale paper in the desired shape. To get the ground truth data, a photo of a fiber laying on a paper was

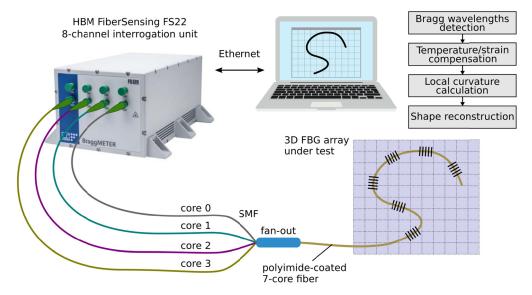


Fig. 4. Measurement system. Interrogation scheme used for FBG resonances detection and tracking.

taken and the shape digitized with a specialized software tool. The 3D spiral had a diameter $D=25\,$ mm and pitch $h=10\,$ mm. The winding of the fiber was done under tension to ensure a snug fit and by following the reference line drawn onto a cylinder surface, whereas the ends of the sensor were sealed with adhesive tape. In this case, as a ground truth data we used the curve obtained from analytical formulas for a 3D spiral.

IV. RESULTS AND DISCUSSION

The shape reconstruction is shown for three different setups, namely a spiral, a bow and an S shape. A previous analysis for similar spiral shapes can be found in [15]. The structure chosen for presenting the results is the following:

- 1) The reconstruction is iterated for both methods for a large number of increasing values of the interpolation factor m, and the average error, i.e. the mean of the Euclidean distances between the reconstructed points and the ground truth, is plotted. By fixing a value for the interpolation factor m it is possible to compare the accuracy of the two algorithms. By choosing a value for the average error it is possible to understand which is the interpolation factor m that is required for the algorithms to provide such result.
- 2) After selecting a value for the interpolation factor *m*, the shape reconstruction is graphically presented. The figure presents a clear view of the results that can be achieved in the two cases.
- 3) The evolution of the curvature modulus and phase is shown so that it is possible to analyse the properties of the shape, such as inflection points, where the modulus tends to zero and the phase exhibits a shift of 180°.
- 4) The evolution of the norm of the three orthonormal versors calculated with the Frenet-Serret equations, i.e., T N and B, is reported. The reconstruction is hindered if the norm of these vectors strays from the unitary value, which is very evident in the case of inflection points in the shapes under study.

5) Lastly, a table reports the relevant data of the experiment, such as the calculated strains and the accuracy and performance of the algorithms. The performance is evaluated, with the MATLAB tic toc function, in terms of average computation time over 1000 instances of the algorithms, and the average refresh rate (calculated as the inverse of the average computation time) gives an idea of the possible reconstruction capabilities in a real-time application. The algorithms were executed sequentially, no multi-thread was applied.

The relevant specifications of the terminal used for the performance analysis are the following: Processor: Intel(R) Core (TM) i7-8565U CPU @ 1.80GHz, 1992 MHz, 4 Core(s), 8 Logical Processor(s), RAM: 8 GB.

Results for the spiral shape with the multicore 6 FBG fiber are reported in Fig. 5 and Table I. The reconstruction is highly accurate since the obtained average errors are sub millimetric, and both algorithms are viable for applications like the medical ones (catheters, flexible endoscopes), where the precision in the reconstructed shape is paramount for a successful procedure [20]. The interpolation factor chosen in Fig. 5b is m = 100; it is the smallest value that minimizes the reconstruction error, and corresponds to 100 segments with a length of 0.14 mm between two consecutive FBGs. The best achievable average error is 0.28 mm; as shown in Fig. 5c, the curvature is not perfectly constant, nor the direction angle is perfectly linear. The evolution of the norms of the TNB triplet is shown in Fig. 5d; although not being unitary, the difference is small enough and the shape can be properly reconstructed with the Frenet-Serret equations. The average error obtained for the spiral shape is comparable with the results obtained in a previous work for similar 3D shapes and sizes, which reports a mean error ranging from 0.12 mm to 0.23 mm [21].

Results for the bow shape with the multicore 6 FBG fiber are reported in Fig. 6 and Table II. The presence of two inflection points in the curve (Fig. 6c) causes the TNB triplet

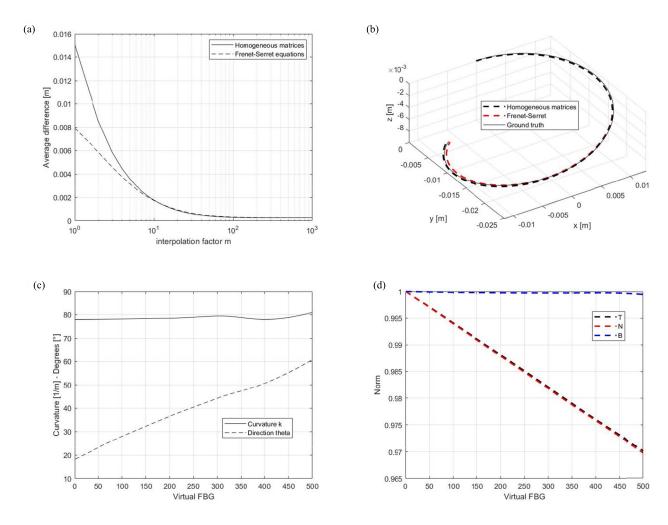


Fig. 5. Spiral–3D. a) Spiral reconstruction, average error - the average distance between the points calculated by the two different algorithms with the same interpolation factor and the ground truth is presented. As the interpolation factor is increased, the difference becomes negligible. b) 3D spiral reconstruction - ground truth (solid line), recovered shape with the proposed method (dashed black line) and recovered shape with Frenet-Serret (dashed red line) are shown. The chosen interpolation factor is m=100 as it provides a trade-off between accuracy and performance. c) Spiral curvature and direction angle - the measured curvature $[m^{-1}]$ (solid line) and the measured curvature direction $[\circ]$ (dashed line) are presented. The almost constant curvature is in accordance with the constant radius of the cylinder and the behavior of the direction angle θ is similar to the linear one of a spiral pitch. d) Norms of the Frenet-Serret versors (spiral) - the evolution of the norms of the TNB triplet is presented. Although not being unitary, the norm is preserved enough to yield a good result. By increasing the interpolation factor m, the decadence maintains its shape but is decreased in amplitude, in accordance with Fig. 5a.

TABLE I
STRAIN VALUES MEASURED FOR SPIRAL SHAPE AND SENSING RESULTS OF THE ALGORITHMS

	Measured strain [$\mu arepsilon$]										
	Node 1	Node 2	Node 3 Node 4		Node 5		Node 6				
Core 1	-970.0	-1033.4	-1062.8	-1069.4	-944.2	2 -1067.3					
Core 2	-2086.0	-2029.1	-2038.6	-2126.0	-2167.0		-2159.4				
Core 3	3107.9	3138.1	3142.3	3139.0	3062.	0	3217.9				
	Homogeneous transformation matrices (H) and Frenet-Serret equations (FS)										
	Interpolation factor m		verage error [mm]	Avg. computation time [s]		Avg. refresh rate [Hz]					
Н	100		0.28	0.0023		435					
FS	100		0.31	0.0032		312					
FS	143		0.28	0.0044		225					

to noticeably lose the unitary norm (Fig. 6d) and compromises the reconstruction (Fig. 6b). The interpolation factor chosen for the reconstruction is m=100, in accordance with the

choice made in the spiral experiment (and corresponding to 100 segments 0.14 mm-long between two successive FBGs centers). The best achievable average error is 0.39 mm.

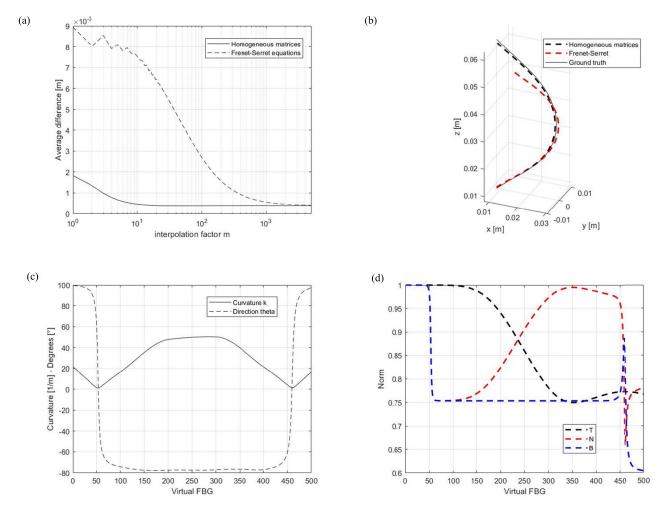


Fig. 6. Bow–2D. a) Bow reconstruction, average error-the average distance between the points calculated by the two different algorithms with the same interpolation factor and the ground truth is presented. Although the difference becomes negligible as the interpolation factor is increased, it is noticeable for all interpolation factors m < 5000. b) 3D bow reconstruction - ground truth (solid line), recovered shape with the proposed method (dashed black line) and recovered shape with Frenet-Serret (dashed red line) are shown. The chosen interpolation factor is m = 100 to be consistent with the choice previously made for the spiral. c) Bow curvature and direction angle - the measured curvature $[m^{-1}]$ (solid line) and the measured curvature direction [°] (dashed line) are presented. The evolution of the curvature direction reflects the double bend of the shape. d) Norms of the Frenet-Serret versors (bow) - the evolution of the norms of the TNB triplet is presented. The double change in direction affects the norm of the TNB triplet, but the algorithm still manages to yield acceptable results for very large interpolation factors, where the norm drop is mitigated in amplitude.

TABLE II
STRAIN VALUES MEASURED FOR THE BOW SHAPE AND SENSING RESULTS OF THE ALGORITHMS

	Measured strain [$\mu arepsilon$]								
	Node 1	Node 2		Node 3	Node 4	Node 5		Node 6	
Core 1	-831.9	711.9	9	1943.0	2004.2	797.2		-583.9	
Core 2	571.7	-386.	2	-834.2	-607.4	-156.	9	-58.0	
Core 3	324.5	-234.	0	-1080.9	-1352.7	-678.	1	623.8	
		Homogeneo	ous transfo	ormation matrices (H) and Frenet-Serret equ	uations (FS)			
	Interpolation factor m Ave		Aver	age error [mm]	Avg. computation time [s]		Avg. refresh rate [Hz]		
Н	100		0.39		0.0023		435		
FS	100		2.70		0.0032		312		
FS	5000		0.39		0.1618		6		

For very large interpolation factors m, the discontinuity in phase is divided in shorter intervals where the difference between two sequential values of the angle becomes acceptable and the Frenet-Serret reconstruction recovers accuracy.

As it can be seen in Fig. 6a, the reconstruction error for Frenet-Serret tends to the same value of the transformation matrices for increasing values of interpolation. In fact, the perturbation of the Frenet-Serret frame shown in Fig. 6d, although

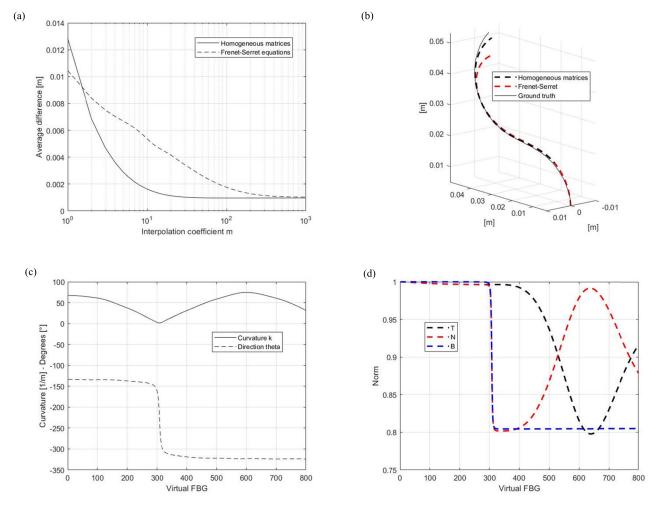


Fig. 7. S-shape–2D. a) S-shape reconstruction, average error-the average distance between the points calculated by the two different algorithms with the same interpolation factor and the ground truth is presented. For increasing interpolation factors m, the error decreases and the Frenet-Serret reconstruction reaches the same output of the presented algorithm. b) 3D s-shape reconstruction - ground truth (solid line), recovered shape with the proposed method (dashed black line) and recovered shape with Frenet-Serret (dashed red line) are shown. The chosen interpolation factor is m=100 to be consistent with the choice previously made for the spiral. c) S-shape curvature and direction angle - the measured curvature $[m^{-1}]$ (solid line) and the measured curvature direction in degrees (dashed line) are presented. The direction angle has been a posteriori modified to prevent arctangent discontinuities from occurring. d) Norms of the Frenet-Serret versors (s-shape) - the evolution of the norms of the TNB triplet is presented.

maintaining its shape, will be scaled down and become negligible. The downside is obviously the computational effort needed to perform the satisfactory level of interpolation on the data. On the other hand, the proposed algorithm is insensitive to discontinuities in the phase and performs well even at low values of interpolation.

Results for the s-shape with the multicore 9 FBG fiber are reported in Fig. 7, as well as in Table III. The difference in accuracy is noticeable, proving that even a single inflection point in the shape hinders the traditional Frenet-Serret reconstruction. As already stated for the previous experiment, a large effort in interpolation can mitigate the intensity of the perturbation and yield results close to the ones obtained with the homogeneous transformation matrices, at the cost of the computational performance. The interpolation factor chosen for the reconstruction is m = 100. In this case, being the distance between nodes equal to 10 mm, the choice of m corresponds to 100 segments (length of each segment is

0.1 mm) between two consecutive FBGs. The best achievable average error with this interpolation factor is 1.00 mm. This last result is comparable with previous data provided in [20], where a average error of 1.15 mm is obtained on a 38 cm catheter, after implementing curvature and angle correction.

The results of the experiments show that the accuracy of the overall sensing system depends on three main factors: the reconstruction algorithm, the multicore fiber under test and the complexity of the forms. Once a fiber is selected, and a desired average reconstruction error threshold is fixed, the choice of the algorithm determines the performance in terms of execution time. The algorithm based on transformation matrices scores better than the traditional Frenet-Serret equations in all the presented cases.

Another important result is that the method based on transformation matrices, with the available hardware, can run at an average frequency of 435 Hz for the 6 FBG array (spiral, bow) and 324 Hz for the 9 FBG array (s-shape).

	Measured strain [$\mu arepsilon$]										
	Node 1	Node 2	Node 3	Node 4	No	de 5	Node 6	Node 7	Node 8	Node 9	
Core 1	1818.1	1458.1	711.4	2.3	-40	6.7	-421.2	-178.4	139.6	181.8	
Core 2	475.0	745.0	678.3	101.6	-88	6.0	-1943.8	-2690.5	-2332.5	-1270.6	
Core 3	-2771.6	-2555.1	-1557.0	-82.3	121	2.6	2143.2	2547.5	1896.4	855.3	
		Homo	geneous transfo	ormation matri	ces (H)	and Fre	net-Serret equa	itions (FS)			
	Interpolation factor m		Aver	Average error [mm]		Avg. computation time [s]		Avg. refresh rate [Hz]			
Н	100			1.00		0.0031		324			
FS	100			1.65		0.0050		201			
FS	1000			1.00		0.0495			20		

TABLE III
STRAIN VALUES MEASURED FOR THE S-SHAPE AND SENSING RESULTS OF THE ALGORITHMS

The Frenet-Serret algorithm, executed with an interpolation factor that allows reaching the same average error obtained with the transformation matrices, scores an average frequency of 225 Hz (spiral, 6 FBG array), 6 Hz (bow, 6 FBG array) and 20 Hz (s-shape, 9 FBG array).

Frenet-Serret equations have been largely investigated as a method for shape reconstruction, and recently compared to other approaches and improved versions, such as Bishop frame [20], [31]. Among the alternative approaches, transformation matrices have demonstrated good performances for 3D shape sensing. A kinematics-based model based on homogeneous transformation was introduced and assessed also in [32], aimed at calculating the deflection of a needle embedding three separated optical fibers. In accordance with the preliminary reports by [20], [22], the method based on transformation matrices has shown better performances than Frenet-Serret equations in 3D shape sensing performed also with the proposed multicore fiber. The present work further investigates the influence of parameters of the algorithms on the performances of the two methods for the shape reconstruction; the results are given for every choice of the interpolation factor and the selected shapes are characterized by high curvatures, while the aforementioned work only focuses on shapes with mild curvatures and for a single choice of parameters. A detailed comparison with the state of the art in terms of both evolution of the accuracy depending on the interpolation factor and computational efforts is given in the present work. Furthermore, the results are shown for two different custom-made multicore fibers in order to prove the uncorrelation between the algorithm properties and the specific fiber under test.

V. CONCLUSION

This work presents a comparison between two different three-dimensional reconstruction algorithms for the estimation of the shape of a multicore fiber optic-based sensing system. The designed multicore fibers allow an accurate measurement of their shape, which makes them suitable for those applications where accuracy is paramount. A non-exhaustive list of potential fields of interest for the application is: medical and industrial robotics, mining industry and aerospace. The algorithm based on transformation matrices is characterized by a better performance in respect to the traditional Frenet-Serret equations, proving to be suitable for applications where

fast real-time feedback is needed; in fact, it is able to provide the same accuracy with lower computational effort, while also being more stable against discontinuities in the measured curvature angle values. Future works will involve developing a real-time application of the algorithm.

REFERENCES

- M. Amanzadeh, S. M. Aminossadati, M. S. Kizil, and A. D. Rakić, "Recent developments in fibre optic shape sensing," *Measurement*, vol. 128, pp. 119–137, Nov. 2018.
- [2] Y.-L. Park et al., "Real-time estimation of 3-D needle shape and deflection for MRI-guided interventions," *IEEE/ASME Trans. Mechatronics*, vol. 15, no. 6, pp. 906–915, Dec. 2010.
- [3] E. M. Boctor, M. A. Choti, E. C. Burdette, and R. J. Webster, Iii, "Three-dimensional ultrasound-guided robotic needle placement: An experimental evaluation," *Int. J. Med. Robot. Comput. Assist. Surg.*, 4, no. 2, pp. 180–191, 2008.
- [4] X. Su and Q. Zhang, "Dynamic 3-D shape measurement method: A review," Opt. Lasers Eng., vol. 48, no. 2, pp. 191–204, Feb. 2010.
- [5] S. Zhang, "Recent progresses on real-time 3D shape measurement using digital fringe projection techniques," *Opt. Lasers Eng.*, vol. 48, no. 2, pp. 149–158, Feb. 2010.
- [6] K. Ohno, T. Nomura, and S. Tadokoro, "Real-time robot trajectory estimation and 3D map construction using 3D camera," in *Proc. IEEE/RSJ Int. Conf. Intell. Robots Syst.*, Oct. 2006, pp. 5279–5285.
- [7] F. Peña, L. Richards, A. R. Parker, Jr., A. Piazza, P. Chan, and P. Hamory, "Fiber Optic Sensing System (FOSS) technology—A new sensor paradigm for comprehensive structural monitoring and model validation throughout the vehicle life-cycle," NASA Armstrong Flight Res. Center, Edwards, CA, USA, Tech. Rep., 2015. [Online]. Available: https://www.nasa.gov/sites/default/files/atoms/files/dr-0001-lst-016-foss-4pgr-online.pdf
- [8] L. Danisch, A. Chrzanowski, J. Bond, and M. F. Bazanowski, "Fusion of geodetic and MEMS sensors for integrated monitoring and analysis of deformations," in *Proc. 13th FIG Int. Symp. Deform. Meas. Anal.*, Lisbon, Portugal, May 2008, pp. 12–15.
- [9] A. Dementyev, H.-L. C. Kao, and J. A. Paradiso, "Sensortape: Modular and programmable 3D-aware dense sensor network on a tape," in *Proc. 28th Annu. ACM Symp. User Interface Softw. Technol.*, 2015, pp. 649–658.
- [10] A. D. Kersey et al., "Fiber grating sensors," J. Lightw. Technol., 15, no. 8, pp. 1442–1462, Aug. 1997.
- [11] E. Udd and W. B. Spillman, Jr., Fiber Optic Sensors: An Introduction for Engineers and Scientists. Hoboken, NJ, USA: Wiley, 2011.
- [12] A. Othonos, K. Kalli, and G. E. Kohnke, "Fiber Bragg gratings: Fundamentals and applications in telecommunications and sensing," *Phys. Today*, vol. 53, no. 5, pp. 61–62, May 2000.
- [13] M. E. Froggatt and R. G. Duncan, "Fiber optic position and/or shape sensing based on Rayleigh scatter," U.S. Patent 7772 541 B2, 2010.
- [14] M. E. Froggatt, J. W. Klein, D. K. Gifford, and S. T. Kreger, "Optical position and/or shape sensing," U.S. Patent 8773 650 B2, 2014.
- [15] K. Bronnikov et al., "Durable shape sensor based on FBG array inscribed in polyimide-coated multicore optical fiber," Opt. Express, vol. 27, no. 26, pp. 38421–38434, 2019.
- [16] M. Froggatt and J. Moore, "High-spatial-resolution distributed strain measurement in optical fiber with Rayleigh scatter," *Appl. Opt.*, vol. 37, no. 10, pp. 1735–1740, 1998.

- [17] A. Masoudi and T. P. Newson, "Contributed review: Distributed optical fibre dynamic strain sensing," *Rev. Scientific Instrum.*, vol. 87, no. 1, Jan. 2016, Art. no. 011501.
- [18] T. Erdogan, "Fiber grating spectra," J. Lightw. Technol., vol. 15, no. 8, pp. 1277–1294, Aug. 1997.
- [19] K. K. C. Lee, A. Mariampillai, M. Haque, B. A. Standish, V. X. D. Yang, and P. R. Herman, "Temperature-compensated fiberoptic 3D shape sensor based on femtosecond laser direct-written Bragg grating waveguides," *Opt. Express*, vol. 21, no. 20, pp. 24076–24086, 2013.
- [20] S. Jäckle, T. Eixmann, H. Schulz-Hildebrandt, G. Hüttmann, and T. Pätz, "Fiber optical shape sensing of flexible instruments for endovascular navigation," *Int. J. Comput. Assist. Radiol. Surg.*, vol. 14, no. 12, pp. 2137–2145, Dec. 2019.
- [21] F. Khan, A. Denasi, D. Barrera, J. Madrigal, S. Sales, and S. Misra, "Multi-core optical fibers with Bragg gratings as shape sensor for flexible medical instruments," *IEEE Sensors J.*, vol. 19, no. 14, pp. 5878–5884, Jul. 2019.
- [22] X. Chen, X. Yi, J. Qian, Y. Zhang, L. Shen, and Y. Wei, "Updated shape sensing algorithm for space curves with FBG sensors," *Opt. Lasers Eng.*, vol. 129, Jun. 2020, Art. no. 106057.
- [23] A. V. Dostovalov, A. A. Wolf, A. V. Parygin, V. E. Zyubin, and S. A. Babin, "Femtosecond point-by-point inscription of Bragg gratings by drawing a coated fiber through ferrule," *Opt. Express*, 24, no. 15, pp. 16232–16237, 2016.
- [24] J. P. Moore and M. D. Rogge, "Shape sensing using multi-core fiber optic cable and parametric curve solutions," *Opt. Express*, vol. 20, no. 3, pp. 2967–2973, 2012.
- [25] C. A. Rabbath and D. Corriveau, "A comparison of piecewise cubic Hermite interpolating polynomials, cubic splines and piecewise linear functions for the approximation of projectile aerodynamics," *Defence Technol.*, vol. 15, no. 5, pp. 741–757, 2019.
- [26] R. S. Esfandiari, Numerical Methods for Engineers and Scientists Using MATLAB, 2nd ed. Boca Raton, FL, USA: CRC Press, 2017.
- [27] J. Cui, S. Zhao, C. Yang, and J. Tan, "Parallel transport frame for fiber shape sensing," *IEEE Photon. J.*, vol. 10, no. 1, pp. 1–12, Feb. 2018.
- [28] J. P. Moore, "Method and apparatus for shape and end position determination using an optical fiber," U.S. Patent 7813599 B2, 2010.
- [29] K. T. V. Gratten and B. T. Meggitt, Optical Fiber Sensor Technology: Applications and Systems, vol. 3. Norwell, MA, USA: Kluwer, 1999.
- [30] A. Wolf, A. Dostovalov, K. Bronnikov, and S. Babin, "Arrays of fiber Bragg gratings selectively inscribed in different cores of 7-core spun optical fiber by IR femtosecond laser pulses," *Opt. Express*, vol. 27, no. 10, pp. 13978–13990 2019.
- [31] F. Khan, A. Donder, S. Galvan, F. R. Y. Baena, and S. Misra, "Pose measurement of flexible medical instruments using fiber Bragg gratings in multi-core fiber," *IEEE Sensors J.*, vol. 20, no. 18, pp. 10955–10962, Sep. 2020.
- [32] R. J. Roesthuis, M. Kemp, J. J. van den Dobbelsteen, and S. Misra, "Three-dimensional needle shape reconstruction using an array of fiber Bragg grating sensors," *IEEE/ASME Trans. Mechatronics*, vol. 19, no. 4, pp. 1115–1126, Aug. 2014.



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